TITLE OF THE INVENTION

      Methods and Apparatus for Measuring Internal
Information of Scattering Medium

RELATED APPLICATION

      This is a continuation-in-part application of
application serial no.PCT/JP99/06181 filed on November
5, 1999, now pending.

BACKGROUND OF THE INVENTION

Field of the Invention

      The present invention relates to methods and
apparatus for measuring internal information of
scattering media, e.g., an absorption coefficient or a
concentration of an absorber.

Related Background Art

      Methods of measuring an absorption coefficient of
a scattering medium being a medium to be measured, a
concentration of an absorber or the like, based on the
Microscopic Beer-Lambert Law (hereinafter referred to
as "MBL law"), include, for example, the methods
disclosed in Japanese Patent Applications Laid-Open No.
H08-94517, No. H10-73481, and No. H10-111238 by the
inventors. These methods based on the MBL law possess
the significant feature of being theoretically free of
the influence of ① the shape of medium, ② boundary
conditions, ③ scattering, and so on, and the same
analytical formulas can be applied to media having any

medium shape, any boundary conditions, and various
scattering characteristics as long as there is no
reentry of photon into the scattering medium.

The measuring methods based on the MBL law can be
roughly classified under four types at present. They
are (1) Time Resolved Spectroscopy (hereinafter
referred to as "TRS method") making use of the time-
resolved profile of re-emission, (2) Time Integrated
Spectroscopy (hereinafter referred to as "TIS method")
making use of the time integral value of the time-
resolved profile of re-emission and the mean pathlength,
(3) Time Gating Spectroscopy (hereinafter referred to
as "TGS method") making use of portions cut out of the
time-resolved profile by gates, and (4) Phase
Modulation Spectroscopy (hereinafter referred to as
"PMS method") making use of modulated light. Among
these, (2) the TIS method and (4) the PMS method
utilizing all re-emission are advantageous from the
viewpoint that optical attenuation due to scattering is
great in living tissues and it is thus important to use
as much re-emission as possible in practical use.
These two measuring methods are in the relation of
Fourier transform with each other.

SUMMARY OF THE INVENTION

While the measuring methods based on the MBL law
have the many advantages as described above, the

2

measurement accuracy thereof, however, is not sufficient yet for utilization and application in the wide range. For example, there was the problem that, in the case of a living tissue being a measured object, various individual differences, such as color of skin, presence/absence of hair, etc., affected the absolute value of light intensity or the like, so as to be the cause of degradation of the measurement accuracy. Further, the wavelength dependence of scattering coefficient also degrades the measurement accuracy.

There was another problem that reduction was insufficient in the computation time of analysis during measurement and it was thus difficult to implement real-time measurement.

The present invention has been accomplished in view of the above problems and an object of the invention is to provide measuring methods and apparatus of internal information of scattering medium capable of measurement with higher accuracy and at higher speed, when compared with the conventional measuring methods based on the MBL law.

The inventor has conducted intensive and extensive research in order to accomplish the above object and finally found that it became feasible to implement highly accurate measurement by measuring the mean pathlength and variance, particularly, for pulsed

light of a plurality of different wavelength components, by the Mean and Variance based Spectroscopy (hereinafter referred to as "MVS method") utilizing the mean pathlength and variance, or physical quantities

5   equivalent thereto, without use of information such as absolute values of light intensity or a ratio thereof, and to readily put the wavelength dependence of scattering coefficient into analytical formulas, thus accomplishing the present invention. Likewise, the

10   inventor found that it also became feasible to implement highly accurate measurement by measuring the group delay for modulated light of a plurality of different wavelength components and the second partial derivative of logarithm of amplitude with respect to

15   modulation frequency, thus accomplishing the present invention.

Specifically, a first measuring method of internal information of a scattering medium according to the present invention is a method comprising (1) a

20   light injecting step of injecting pulsed light of two or more predetermined wavelengths into a scattering medium at a light injection position, (2) a light detecting step of detecting the light of the two or more predetermined wavelengths having propagated inside

25   the scattering medium, at a photodetection position to acquire a photodetection signal, (3) a signal

4

processing step of acquiring waveform data indicating a
temporal change of intensity of the detected light,
based on the photodetection signal, (4) a mean
pathlength and variance computing step of performing an
5   operation to compute a mean pathlength of plural
photons composing the detected light, and a variance,
based on the waveform data, and (5) an absorption
coefficient difference calculating step of calculating
a difference between absorption coefficients at the
10   predetermined wavelengths, based on a predetermined
relation holding among the mean pathlength, the
variance, and the difference between the absorption
coefficients at the two or more predetermined
wavelengths.

15   A first measuring apparatus of internal
information of a scattering medium according to the
present invention is an apparatus comprising (1) light
injecting means for injecting pulsed light of two or
more predetermined wavelengths into a scattering medium
20   at a light injection position, (2) light detecting
means for detecting the light of the two or more
predetermined wavelengths having propagated inside the
scattering medium, at a photodetection position to
acquire a photodetection signal, (3) signal processing
25   means for acquiring waveform data indicating a temporal
change of intensity of the detected light, based on the

photodetection signal, (4) mean pathlength and variance computing means for performing an operation to compute a mean pathlength of plural photons composing the detected light, and a variance, based on the waveform data, and (5) absorption coefficient difference calculating means for calculating a difference between absorption coefficients at the predetermined wavelengths, based on a predetermined relation holding among the mean pathlength, the variance, and the difference between the absorption coefficients at the two or more predetermined wavelengths.

The above first method and apparatus according to the present invention are based on a TIMVS method, which is an MVS method in which the analysis is carried out in the time domain by the time integrated spectroscopy (TIS method). The TIMVS method using the mean pathlength and variance for the light of plural wavelength components in this way presents very significant advantages in practical use, including ① being not influenced by the individual differences and absolute values of intensity of incident light dependent upon wavelengths and positions, ② extremely simplifying the quantitative formula involving the wavelength dependence of scattering coefficient, ③ decreasing errors in determination of the zero point (t = 0) of the time axis in the time-resolved spectroscopy,

6

and so on, in addition to the advantages presented by the conventional measuring methods based on the MBL law.

In the method and apparatus, it also becomes feasible to greatly reduce the measurement and analysis time and implement real-time measurement, by applying the Simple Subtraction Method (SSM) developed by the inventors, which permits the mean pathlength of detected photons (the center of gravity of a time-resolved profile) and the variance to be computed at high speed by calculating the moment of the time-resolved profile with a computer. This SSM is described, for example, in Japanese Patent Application Laid-Open No. H09-61343.

A second measuring method of internal information of a scattering medium according to the present invention is a method comprising (1) a light injecting step of injecting modulated light of two or more predetermined wavelengths modulated at a predetermined frequency, into a scattering medium at a light injection position, (2) a light detecting step of detecting the light of the two or more predetermined wavelengths having propagated inside the scattering medium, at a photodetection position to acquire a photodetection signal, (3) a signal processing step of extracting a signal of the predetermined frequency component from the photodetection signal, (4) a group

delay and second-partial-derivative-of-logarithm-of-amplitude computing step of computing a group delay of the signal of the predetermined frequency component and a second partial derivative of logarithm of amplitude with respect to the modulation frequency, based on the signal of the predetermined frequency component, and (5) an absorption coefficient difference calculating step of calculating a difference between absorption coefficients at the predetermined wavelengths, based on a predetermined relation holding among the group delay, the second partial derivative of logarithm of amplitude with respect to the modulation frequency, and the difference between the absorption coefficients at the two or more predetermined wavelengths.

A second measuring apparatus of internal information of a scattering medium according to the present invention is an apparatus comprising (1) light injecting means for injecting modulated light of two or more predetermined wavelengths modulated at a predetermined frequency, into a scattering medium at a light injection position, (2) light detecting means for detecting the light of the two or more predetermined wavelengths having propagated inside the scattering medium, at a photodetection position to acquire a photodetection signal, (3) signal processing means for extracting a signal of the predetermined frequency

8

component from the photodetection signal, (4) group delay and second-partial-derivative-of-logarithm-of-amplitude computing means for computing a group delay of the signal of the predetermined frequency component

5   and a second partial derivative of logarithm of amplitude with respect to the modulation frequency, based on the signal of the predetermined frequency component, and (5) absorption coefficient difference calculating means for calculating a difference between

10   absorption coefficients at the prescribed wavelengths, based on a predetermined relation holding among the group delay, the second partial derivative of logarithm of amplitude with respect to the modulation frequency, and the difference between the absorption coefficients

15   at the two or more predetermined wavelengths.

The above-described second method and apparatus according to the present invention are based on a PMMVS method, which is an MVS method in which the analysis is carried out in the frequency domain by the phase

20   modulation spectroscopy (PMS method). This PMMVS method is in the relation of Fourier transform with the TIMVS method associated with the first method and apparatus according to the present invention, and the PMMVS method using the group delay and the second

25   partial derivative of logarithm of amplitude with respect to the modulation frequency for the light of

9

the plural wavelengths in this way presents very significant advantages in practical use, including the aforementioned advantages ①, ② described as to the TIMVS method, and ④ decreasing errors in determination of the zero point of the phase in the phase modulation spectroscopy, and so on, in addition to the advantages provided by the conventional measuring methods based on the MBL law.

BRIEF DESCRIPTION OF THE DRAWINGS

Fig. 1 is a graph to show the relationship between mean pathlength and absorption coefficient for different scattering coefficients.

Fig. 2 is a schematic diagram to show an embodiment of the measuring apparatus of internal information of scattering medium according to the present invention.

Fig. 3 is a schematic diagram to show an example of preferred specific structure of the apparatus illustrated in Fig. 2.

Fig. 4 is a flowchart to show an embodiment of the measuring method of internal information of scattering medium according to the present invention.

Fig. 5 is a flowchart to show another embodiment of the measuring method of internal information of scattering medium according to the present invention.

Fig. 6 is a schematic diagram to show another

embodiment of the measuring apparatus of internal information of scattering medium according to the present invention.

Fig. 7 is a schematic diagram to show an example of preferred specific structure of the apparatus illustrated in Fig. 6.

Fig. 8 is a graph to show absorption spectra of hemoglobin.

Fig. 9 is a graph to show the relationship between absorption coefficient and mean pathlength of a phantom.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

Detailed below with reference to the drawings are preferred embodiments of the measuring methods and apparatus of internal information of scattering medium according to the present invention. In the description of the drawings the same elements will be denoted by the same reference symbols and redundant description will be omitted.

First, the principles of the present invention will be described.

(Principles of the invention)

Calculation of absorption coefficient difference by TIS method

The survival probability of photons propagating in a zigzag path inside a scattering medium is the

exponential of the product of the zigzag pathlength l and the scattering coefficient μ_a of the medium (scattering medium), exp(-μ_al). Namely, the attenuation is expressed by the product μ_al of the zigzag photon pathlength l and the absorption coefficient μ_a. At this time, the impulse response h(t) of the scattering medium is a time-causal function, which is expressed as follows.

$$h(t) = h(\mu_s, \mu_a, t) = s(\mu_s, t)\exp(-\mu_a ct) \qquad (1.1a)$$

$$\frac{\partial}{\partial \mu_a}\ln h(\mu_s, \mu_a, t) = -ct = -\ell \qquad (1.1b)$$

$$\ln h(t) = \ln s(\mu_s, t) - \int_0^{\mu_a} \ell d\mu = \ln s(\mu_s, t) - \mu_a \ell \qquad (1.1c)$$

Here μ_s and μ_a represent an anisotropic scattering coefficient and an absorption coefficient, c the speed of photons in the medium, t the time of flight, and l the photon pathlength (distance of flight). The function s(μ_s,t) is the response at the absorption coefficient μ_a = 0. The time of flight t can be measured by time-resolved spectroscopy. The speed of photons c is determined by the refractive index of the scattering medium and can be deemed as a constant, for example, in the case of living tissues. The above facts are called the MBL law. A transport scattering coefficient μ'_s (also called an equivalent scattering coefficient) used hereinafter is expressed as μ'_s = (1 - g)μ_s, using μ_s and an average g of cosine of

12

scattering angles.

The temporal integration I(μ_s,μ_a) of the impulse response h(t) of the scattering medium is given as follows.

$$I(\mu_s,\mu_a)=\int_0^\infty s(\mu_s,t)\exp(-\mu_a ct)dt \qquad (1.2a)$$

5

$$\frac{\partial \ln I(\mu_s,\mu_a)}{\partial \mu_a}=-c\frac{\int_0^\infty t\,s(\mu_s,t)\exp(-\mu_a ct)dt}{\int_0^\infty s(\mu_s,t)\exp(-\mu_a ct)dt}=-c\langle t\rangle=-\langle \ell\rangle=-L(\mu_s,\mu_a) \quad (1.2b)$$

$$\ln I(\mu_s,\mu_a)=-\int_0^{\mu_a} L(\mu_s,\mu)d\mu+\ln\int_0^\infty s(\mu_s,t)dt \qquad (1.2c)$$

L(μ_s,μ_a) = c<t> in above Eq. (1.2b) represents an average of pathlengths of detected photons (which is also called a mean pathlength). On this occasion, <t> indicates the center of gravity of the impulse response

10   profile (mean time of flight of detected photons) and can be readily calculated by an operation with a computer (to compute the moment) from the temporal profile of the impulse response.

Next, absorption coefficient dependency of the

15   mean pathlength L(μ_s,μ_a) is derived as follows.

$$\frac{\partial L(\mu_s,\mu_a)}{\partial \mu_a}=-\frac{\int_0^\infty (\ell-\langle\ell\rangle)^2 s(\mu_s,t)\exp(-\mu_a ct)dt}{\int_0^\infty s(\mu_s,t)\exp(-\mu_a ct)dt}=-\left[\langle\ell^2\rangle-\langle\ell\rangle^2\right]=-\sigma^2(\mu_s,\mu_a) \quad (1.3)$$

Here σ^2 represents the variance of pathlength 1, which is equivalent to a result of partially differentiating the mean pathlength L(μ_s,μ_a) with respect to μ_a and

20   flipping the sign, or to the second partial derivative

of the temporal integration $I(\mu_s, \mu_a)$ with respect to μ_a. This variance $\sigma^2(\mu_s, \mu_a)$ can be readily calculated by an operation with a computer from the temporal profile of the impulse response, similarly as in the case of the

5   above mean pathlength $L(\mu_s, \mu_a)$.

Likewise, we can find the third partial derivative of the temporal integration $I(\mu_s, \mu_a)$ with respect to μ_a, i.e., the second partial derivative of the mean pathlength $L(\mu_s, \mu_a)$ with respect to μ_a, and

10   this value provides information about profile distortion. From the mathematical aspect, if there exists the mth partial derivative, there always exist the (m – 1)th and lower partial derivatives.

Here, assuming that the scattering coefficient μ_s

15   is a constant, the Taylor expansion of the mean pathlength $L(\mu_s, \mu_a) = L(\mu_a)$ around μ_{a1} is expressed as follows.

$$L(\mu_{a1} + \delta) = L(\mu_{a1}) + \delta L'(\mu_{a1}) + \frac{1}{2!}\delta^2 L''(\mu_{a1}) + \cdots\cdots \quad (1.4)$$

In this equation, L' and L" represent the first and

20   second partial derivatives of L with respect to μ_a. Substituting $\delta = \mu_{a2} - \mu_{a1}$ into the above equation, we obtain the following.

$$L(\mu_{a1}) - L(\mu_{a2}) = \delta\sigma^2(\mu_{a1}) - \frac{1}{2}\delta^2 L''(\mu_{a1}) - \cdots\cdots$$

$$\approx (\mu_{a2} - \mu_{a1})\frac{\sigma^2(\mu_{a1}) + \sigma^2(\mu_{a2})}{2} \qquad (1.5)$$

This means that with the scattering coefficient being constant, a change of absorption coefficient (absorption coefficient difference), $(\mu_{a2} - \mu_{a1})$, can be calculated using the mean pathlength of the impulse response (the center of gravity of the time-resolved profile) and the variance. This novel finding will be applied to the measurement of concentration of absorber as described hereinafter.

Temporal widths of incident light pulses used in measurement are finite and bandwidths of amplifiers and counting circuits are also finite. Therefore, the temporal profile (observed waveform or observed values) obtained in actual measurement is the convolution between the impulse response of the scattering medium and the impulse response of the measuring system (also called an instrumental function).

There are two approaches below as means for determining the true mean pathlength and variance of the impulse response of the scattering medium by eliminating the influence of characteristics of the measuring apparatus from measured values. The first approach is the deconvolution method known well. This is a method of obtaining the impulse response by

15

deconvolution of the measured values with the instrumental function and then determining the mean pathlength and variance from the resultant profile. The second approach is a method of separately

5   determining the mean pathlength and variance in the instrumental function and the mean pathlength and variance in the observed profile and then finding the mean pathlength and variance of the impulse response of the scattering medium from these values. In this case,

10   each of the mean pathlength and variance in the impulse response is given by a difference between corresponding values in the observed profile and in the instrumental function.

The observed profile o(t) is expressed as follows,

15   using the impulse response (true re-emission profile) h(t) of the medium and the impulse response of the measuring system (instrumental function) i(t).

$$o(t) = i(t) \otimes h(t) \qquad (2.1)$$

In the equation the symbol $\otimes$ represents the

20   convolution operation. Let μ_o, μ_i, and μ_h denote centers of gravity of the profiles o(t), i(t), and h(t), respectively, and σ_o^2, σ_i^2, and σ_h^2 denote their respective variances. Let us define generating functions of the above respective profiles as follows.

$$H(s) = \int_{-\infty}^{\infty} h(t) \exp(st) dt \qquad (2.2)$$

$$I(s) = \int_{-\infty}^{\infty} i(t) \exp(st) dt \qquad (2.3)$$

$$O(s) = \int_{-\infty}^{\infty} o(t) \exp(st) dt \qquad (2.4)$$

This definition permits these generating functions to be differentiated any times at s = 0.

With these generating functions, the convolution of the profiles can be expressed by the product of the generating functions, i.e., as follows.

$$O(s) = I(s)H(s) \qquad (2.5)$$

The center of gravity μ_o of o(t) is given as follows.

$$\mu_o = \frac{O'(0)}{O(0)} \qquad (2.6)$$

Since the following relation is derived from Eq. (2.5):

$$O'(s) = I'(s)H(s) + I(s)H'(s) \qquad (2.7),$$

we obtain the following relation therefrom.

$$\mu_o = \mu_i + \mu_h \qquad (2.8)$$

Since the variance is given by the following equation:

$$\sigma^2 = \frac{O''(0)}{O(0)} - \left(\frac{O'(0)}{O(0)}\right)^2 \qquad (2.9),$$

we can derive the following relation therefrom.

$$\sigma_o{}^2 = \sigma_i{}^2 + \sigma_h{}^2 \qquad (2.10)$$

Likewise, similar relations are also attained as to the

third and higher moments. Accordingly, each moment for
the impulse response can be quickly calculated with a
computer from the preliminarily measured instrumental
function and the observed profile of the medium.

5   The procedures described above are the approach
of determining the mean pathlength and variance of the
impulse response and the absorption coefficient
difference from the measured profile by the TIS method.

<u>Calculation of absorption coefficient difference by PMS</u>

10   <u>method</u>

      Next described is the measuring method using
intensity-modulated light. The system function H(ω)
indicating the frequency response of the medium is
expressed by the Fourier transform of the impulse

15   response h(t) as follows.

$$H(\omega) = \int_0^\infty h(t)\exp(-j\omega t)dt$$

$$= \int_0^\infty s(\mu_s,t)\exp[-(c\mu_a + j\omega)t]dt$$

$$= R(\mu_s,\mu_a,\omega) + jX(\mu_s,\mu_a,\omega)$$

$$= A(\mu_s,\mu_a,\omega)\exp[-j\phi(\mu_s,\mu_a,\omega)] \qquad (3.1)$$

In this equation R and X represent the real part and
imaginary part, respectively, A and φ the amplitude and
phase delay, respectively, and these can be readily

20   measured by a lock-in amplifier or the like.

      Then the following relations (the Cauchy-Riemann

equations) hold.

$$\frac{\partial R(\mu_s,\mu_a,\omega)}{\partial c\mu_a}=\frac{\partial X(\mu_s,\mu_a,\omega)}{\partial \omega} \qquad (3.2a)$$

$$\frac{\partial R(\mu_s,\mu_a,\omega)}{\partial \omega}=-\frac{\partial X(\mu_s,\mu_a,\omega)}{\partial c\mu_a} \qquad (3.2b)$$

Thus it is seen that the system function H(ω) is a regular function. From Eqs. (3.2a) and (3.2b), we can further derive the following relations.

$$\frac{\partial \ln A(\mu_s,\mu_a,\omega)}{\partial c\mu_a}=-\frac{\partial \phi(\mu_s,\mu_a,\omega)}{\partial \omega} \qquad (3.2c)$$

$$\frac{\partial \ln A(\mu_s,\mu_a,\omega)}{\partial \omega}=\frac{\partial \phi(\mu_s,\mu_a,\omega)}{\partial c\mu_a} \qquad (3.2d)$$

Then we can derive the following equation, for example, from Eq. (3.2c).

$$\ln A(\mu_s,\mu_a,\omega)=-c\int_0^{\mu_a}\frac{\partial \phi(\mu_s,\mu_a,\omega)}{\partial \omega}d\mu+\ln A(\mu_s,0,\omega) \quad (3.3)$$

This Eq. (3.3) is similar to aforementioned Eq. (1.2c) and the left side of Eq. (3.3) is observable. The integrand in the first term of the right side is the group delay and corresponds to the mean pathlength $L(\mu_s,\mu_a)$ described previously. This group delay is approximated as follows, using the phase delays ϕ_1 and ϕ_2 at two modulation frequencies ω_1 and ω_2.

$$\frac{\partial \phi(\mu_s,\mu_a,\omega)}{\partial \omega}=\frac{\phi_2-\phi_1}{\omega_2-\omega_1} \qquad (3.4)$$

The second term of the right side in Eq. (3.3) is a

value at the absorption coefficient $\mu_a = 0$. Further, the group delay $\partial\phi(\mu_s, \mu_a, \omega)/\partial\omega$ can be approximated as follows when $\omega \ll c\mu_a$.

$$\frac{\partial\phi(\mu_s, \mu_a, \omega)}{\partial\omega} = \frac{\phi}{\omega}$$

5   Here ϕ/ω represents the phase delay.

We can obtain the absorption coefficient dependency of the group delay as follows.

$$\frac{\partial}{\partial\mu_a}\frac{\partial\phi(\mu_s, \mu_a, \omega)}{\partial\omega} = -\frac{1}{c}\frac{\partial^2 \ln A(\mu_s, \mu_a, \omega)}{\partial\mu_a^2} = c\frac{\partial^2 \ln A(\mu_s, \mu_a, \omega)}{\partial\omega^2} \quad (3.5)$$

Here $\partial^2 \ln A/\partial\omega^2$ in the right side of Eq. (3.5) can be
10   readily measured using three modulation frequencies. This corresponds to the variance previously defined.

In the above discussion Eq. (3.3) to Eq. (3.5) were obtained from Eq. (3.2c), but it is also possible to obtain similar relations from Eqs. (3.2a), (3.2b),
15   and (3.2d). The PMS method normally obviates the need for the aforementioned deconvolution operation for obtaining the true profile.

Just as in the case of the TIS method, the relation between the group delay and the change of
20   absorption coefficient (absorption coefficient difference) is obtained as follows, assuming that the scattering coefficient μ_s is a constant.

$$\frac{\partial \phi}{\partial \omega}\bigg|_{\mu_{a1}} - \frac{\partial \phi}{\partial \omega}\bigg|_{\mu_{a2}} \approx \frac{c}{2}(\mu_{a2} - \mu_{a1})\left(\frac{\partial^2 \ln A}{\partial \omega^2}\bigg|_{\mu_{a1}} + \frac{\partial^2 \ln A}{\partial \omega^2}\bigg|_{\mu_{a2}}\right) \qquad (3.6)$$

Accordingly, it is also feasible to calculate the change of absorption coefficient (absorption coefficient difference) with the scattering coefficient being constant, from actually measured values of the group delay and the absorption coefficient dependency by the PMS method, similarly as in the case of the aforementioned TIS method.

Calculation of absorber concentration by MVS method

Next described is the mean and variance based spectroscopy (MVS method) to quantify the absorber concentration from values of the mean pathlength and variance of the impulse response. In the following, the transport scattering coefficient $\mu'_s (= (1 - g)\mu_s)$, which is easier to measure in general, is used instead of the scattering coefficient μ_s. For easier description, we will consider dual-wavelength spectroscopy of a scattering medium containing one absorber component and the principal component of water, the wavelengths used in the measurement are λ_1 and λ_2, and the optical constants at the respective wavelengths will be accompanied by subscripts 1 and 2, respectively. At this time, the following relations hold between the concentration C of the absorber and the absorption

coefficients μ_{a1} and μ_{a2} of the medium at the wavelengths λ_1 and λ_2.

$$\mu_{a1} = C\varepsilon_1 + \mu_{w1}, \quad \mu_{a2} = C\varepsilon_2 + \mu_{w2} \qquad (4.1a)$$

$$C = \frac{1}{\varepsilon_2 - \varepsilon_1}[(\mu_{a2} - \mu_{a1}) - (\mu_{w2} - \mu_{w1})] \qquad (4.1b)$$

Here ε_1 and ε_2 indicate extinction coefficients (or
5   absorption coefficients) for unit concentration of the
absorber at the wavelengths λ_1 and λ_2, which are, for
example, molar extinction coefficients for example, and
μ_{w1} and μ_{w2} represent absorption coefficients of water
at the wavelengths λ_1 and λ_2. Therefore, it is possible
10   to quantify the concentration C of the absorber by
obtaining the difference $(\mu_{a2} - \mu_{a1})$ between the
absorption coefficients from measured profiles.

In execution of the above spectroscopy, ordinary
media demonstrate different values of scattering
15   coefficients at the two wavelengths $(\lambda_1$ and $\lambda_2)$. Then
this difference between the scattering coefficients
complicates the algorithm for quantification of the
absorber concentration. In the following we will first
find a relation between the mean pathlength and the
20   transport scattering coefficient and then explain a new
method of quantifying the absorber concentration by use
of the relation.

According to the photon diffusion equation, the
mean pathlength $L(\mu'_s, \mu_a)$ in the case of reflection

measurement, which will be simply abbreviated as L_ρ, is expressed as follows.

$$L_\rho = \frac{3\mu'_s}{2} \frac{r^2}{1+\rho\mu_{eff}} \qquad (4.2a)$$

$$\mu_{eff} = (3\mu'_s \mu_a)^{1/2} \qquad (4.2b)$$

The symbol ρ indicates the source-detector distance, the distance between a light injection position and a photodetection position.

Now let us consider a ratio of mean pathlengths in a case wherein the absorption coefficients are equal, μ_a, but the transport scattering coefficients are μ'_{s1} and μ'_{s2} (which are equal just to the transport scattering coefficients at the wavelengths λ_1 and λ_2) (though this will not usually occur). The ratio is given as follows.

$$\frac{L_\rho(\mu_{s2}, \mu_a)}{L_\rho(\mu_{s1}, \mu_a)} = \frac{\mu'_{s2}}{1+\rho\mu_{eff2}} \frac{1+\rho\mu_{eff1}}{\mu'_{s1}} \qquad (4.3)$$

Here μ_{eff} represents an effective attenuation coefficient and is given as follows.

$$\mu_{eff1} = (3\mu'_{s1} \mu_a)^{1/2}, \qquad \mu_{eff2} = (3\mu'_{s2} \mu_a)^{1/2} \qquad (4.4)$$

However, a photon diffusion constant independent of the absorption coefficient was used herein. When the measurement conditions are ordinary conditions, i.e., ρ > 20 mm, μ'_s > 0.8 mm, and $\mu_a \gg 0.001$ mm^{-1}, Eq. (4.3) is

23

approximated as follows.

$$\frac{L_\rho(\mu_{s2}, \mu_a)}{L_\rho(\mu_{s1}, \mu_a)} = \left(\frac{\mu'_{s2}}{\mu'_{s1}}\right)^{1/2} \qquad (4.5)$$

Namely, the ratio of mean pathlengths in the case wherein the absorption coefficients are equal but the transport scattering coefficients are different is a constant determined by a ratio of the transport scattering coefficients, independent of the absorption coefficients. Since in the measurement of actual media change of the transport scattering coefficient with change of wavelength normally also varies the absorption coefficient, it is difficult to directly measure the ratio of L_ρ represented by Eq. (4.3).

The approximation of Eq. (4.5) also holds similarly for the ratio of mean pathlengths under almost equal conditions to the above, i.e., in the case of ordinary transmission measurement. Fig. 1 schematically shows by L_1 and L_2, an example of the relation between the mean pathlength L and the absorption coefficient μ_a for different transport scattering coefficients.

Eq. (4.5) above is the relation obtained based on the photon diffusion approximation, but the validity of this relation for actual media was proved by the Monte Carlo calculation to simulate scattering media and by

experiments with a tissue-like phantom.

To generalize the above, the ratio of mean pathlengths at the wavelengths λ_1 and λ_2 is approximated as follows and defined by k'.

5

$$\frac{L_2(\mu_a)}{L_1(\mu_a)} \equiv \frac{L(\mu_{s2},\mu_a)}{L(\mu_{s1},\mu_a)} = \left(\frac{\mu'_{s2}}{\mu'_{s1}}\right)^{1/2} \equiv k' \qquad (4.6)$$

$L_1(\mu_a)$ and $L_2(\mu_a)$ used herein indicate the mean pathlengths for a medium having different transport scattering coefficients but an absorption coefficient of an equal value μ_a. Accordingly, use of the

10 coefficient k' defined here permits the ratio of mean pathlengths to be estimated for the medium having the absorption coefficient of the equal value μ_a and the different transport scattering coefficients (see Fig. 2). Moreover, since the fact that Eq. (4.6) holds

15 means that curves representing the mean pathlengths, k' $\times L_1(\mu_a)$ and $L_2(\mu_a)$, are laid on each other on the plane (μ_a, L), the following relation holds for the variances $\sigma^2(\mu'_{s1},\mu_a)$ and $\sigma^2(\mu'_{s2},\mu_a)$ at μ_a of the curves $L_1(\mu_a)$ and $L_2(\mu_a)$ indicating the mean pathlengths.

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$$\sigma^2(\mu'_{s2},\mu_a) \equiv \sigma_2^{\,2}(\mu_a) = k'\sigma^2(\mu'_{s1},\mu_a) \equiv k'\sigma_1^{\,2}(\mu_a) \qquad (4.7)$$

The above knowledge is very significant in the following sense. Namely, use of the coefficient k' defined in Eq. (4.6) permits us to normalize the mean pathlength $L(\mu'_s,\mu_a)$ for media with different transport

scattering coefficients. As a consequence, we can unitarily handle the mean pathlengths for the media with different transport scattering coefficients.

Now let us describe how to determine the concentration C of the absorber, using this relation.

The introduction of the coefficient k' as described above reduces the spectroscopy of the media exhibiting the wavelength dependence of the transport scattering coefficient to measurement of concentration of absorber with the transport scattering coefficient being constant. As a result, we need only to consider one curve indicating the mean pathlength on the plane (μ_a, L) and can apply Eq. (1.5) to the measurement of absorber concentration. Now, referring to Eq. (1.5) with use of the mean pathlength $L_2 = k'L_1$ normalized by k', the following relation holds as to the difference between absorption coefficients.

$$L_2(\mu_{a1}) - L_2(\mu_{a2}) = (\mu_{a2} - \mu_{a1})\frac{\sigma_2^2(\mu_{a1}) + \sigma_2^2(\mu_{a2})}{2}$$

Since there are the following relations:

$$L_2(\mu_{a1}) = L(\mu'_{s2}, \mu_{a1}) = k'L(\mu'_{s1}, \mu_{a1}) = k'L_1(\mu_{a1})$$

$$\sigma_2^2(\mu_{a1}) = \sigma^2(\mu'_{s2}, \mu_{a1}) = k'\sigma^2(\mu'_{s1}, \mu_{a1}) = k'\sigma_1^2(\mu_{a1})'$$

the following relation finally holds.

$$k'L_1(\mu_{a1}) - L_2(\mu_{a2}) = (\mu_{a2} - \mu_{a1})\frac{k'\sigma_1^2(\mu_{a1}) + \sigma_2^2(\mu_{a2})}{2} \quad (4.8)$$

26

This means that the absorption coefficient difference can be quantified using the mean pathlengths $L_1(\mu_{a1})$, $L_2(\mu_{a2})$ and the variances $\sigma_1^2(\mu_{a1})$, $\sigma_2^2(\mu_{a2})$, which are obtained from measured values.

From the above, the absorber concentration C is finally obtained as follows.

$$C = \frac{1}{\varepsilon_2 - \varepsilon_1}\left[\frac{2[k'L_1(\mu_{a1}) - L_2(\mu_{a2})]}{k'\sigma_1^2(\mu_{a1}) + \sigma_2^2(\mu_{a2})} - (\mu_{w2} - \mu_{w1})\right] \qquad (4.9)$$

This yields the equation for quantifying the absorber concentration C by dual-wavelength spectroscopy. Since the mean pathlength term is $(k'L_1 - L_2)$ herein, the problem of error in determination of the zero point of the time axis $(t = 0)$ in time-resolved spectroscopy is largely relaxed in comparison with $(L_1 + L_2)$ in the conventional method. This effect is particularly great in the case of living tissues with $\mu'_s \doteqdot 1$.

In the case of the phase modulation spectroscopy (PMS method), the concentration is given as follows in the same manner as above.

$$C = \frac{1}{\varepsilon_2 - \varepsilon_1}\left[\frac{2[k'\phi_1'(\mu_{a1}) - \phi_2'(\mu_{a2})]}{c[k'\ln A_1''(\mu_{a1}) + \ln A_2''(\mu_{a2})]} - (\mu_{w2} - \mu_{w1})\right] \qquad (4.10)$$

However, the notation follows the following definition.

$$\varphi_1'(\mu_{a1}) = \frac{\partial \phi(\mu'_{s1}, \mu_a)}{\partial \omega}\bigg|_{\mu_{a1}} \quad , \quad \ln A_1''(\mu_{a1}) = \frac{\partial^2 \ln A(\mu'_{s1}, \mu_a)}{\partial \omega^2}\bigg|_{\mu_{a1}}$$

$$\varphi_2'(\mu_{a2}) = \frac{\partial \phi(\mu'_{s2}, \mu_a)}{\partial \omega}\bigg|_{\mu_{a2}} \quad , \quad \ln A_2''(\mu_{a2}) = \frac{\partial^2 \ln A(\mu'_{s2}, \mu_a)}{\partial \omega^2}\bigg|_{\mu_{a2}} \quad (4.11)$$

Since the group delay term is also $(k'\phi'_1 - \phi'_2)$ in
above Eq. (4.10), the problem of error in determination
of the zero point of the phase ($\phi = 0$) in the phase

5   modulation spectroscopy is largely relaxed in
comparison with ($\phi_1 + \phi_2$) in the conventional method.
This effect is also particularly great in the case of
the living tissues with $\mu'_s \doteqdot 1$, as above.

        It is apparent from the above that the

10   spectroscopy (MVS method) according to the present
invention with use of the mean pathlength and variance,
or physical quantities equivalent thereto, presents
tremendous advantages, including ① there will arise no
problem from the individual differences and the

15   absolute value of incident photon intensity dependent
upon the wavelength and position, ② the quantitative
equation is very simple with inclusion of the
wavelength dependency of scattering coefficient, ③ the
problem of error is relaxed in the determination of the

20   zero point of the time axis ($t = 0$) in the time-
resolved spectroscopy, ④ the problem of error is
relaxed in the determination of the zero point of the
phase in the phase modulation spectroscopy, and so on,

28

in addition to those of the conventional measuring methods based on the MBL law.

Eq. (4.8) above can also be derived as follows. First, the following is yielded from Eq. (1.3).

$$L(\mu'_s, \mu_{a1}) = -\int_0^{\mu_{a1}} \sigma^2(\mu_s, \mu_a) d\mu_a + L(\mu_{s1}, 0) \qquad (A.1)$$

Then the difference between mean pathlengths at the wavelengths λ_1 and λ_2 is given as follows.

$$L(\mu'_{s1}, \mu_{a1}) - L(\mu'_{s2}, \mu_{a2})$$
$$= \int_0^{\mu_{a2}} \sigma^2(\mu_{s2}, \mu_a) d\mu_a - \int_0^{\mu_{a1}} \sigma^2(\mu_{s1}, \mu_a) d\mu_a - L(\mu_{s2}, 0) + L(\mu_{s1}, 0) \quad (A.2)$$

Assuming Eq. (4.6) and Eq. (4.7), the following relation is obtained.

$$L(\mu'_{s1}, \mu_{a1}) - L(\mu'_{s2}, \mu_{a2})$$
$$= (k'-1)\int_0^{\mu_{a1}} \sigma^2(\mu_{s1}, \mu_a) d\mu_a + \int_{\mu_{a1}}^{\mu_{a2}} \sigma^2(\mu_{s2}, \mu_a) d\mu_a - (k'-1)L(\mu_{s1}, 0)$$
$$= -(k'-1)L(\mu'_{s1}, \mu_{a1}) + \int_{\mu_{a1}}^{\mu_{a2}} \sigma^2(\mu_{s2}, \mu_a) d\mu_a$$

As a result, aforementioned Eq. (4.8b), i.e., the following equation is derived.

$$k'L_1(\mu_{a1}) - L_2(\mu_{a2}) = (\mu_{a2} - \mu_{a1})\frac{k'\sigma_1^2(\mu_{a1}) + \sigma_2^2(\mu_{a2})}{2} \qquad (4.8b)$$

Next described is a method of quantifying the ratio of transport scattering coefficients. The mean pathlength $L_p(\mu'_s, \mu_a)$ in the reflection measurement is given by aforementioned Eq. (4.2) and is rewritten as

follows by abbreviating it as L.

$$L = \frac{3\mu'_s}{2} \frac{r^2}{1 + \rho\mu_{eff}} \qquad (5.1a)$$

$$\mu_{eff} = (3\mu'_s\mu_a)^{1/2} \qquad (5.1b)$$

In the equation ρ represents the source-detector distance. Thus the variance σ^2 is yielded as follows.

$$\sigma^2 = \frac{\partial^2 \ln I}{\partial \mu_a^2} = -\frac{\partial L}{\partial \mu_a} = \frac{L^2}{\rho\mu_{eff}} \qquad (5.2)$$

Then we obtain the following equations for the transport scattering coefficient μ'_s and the absorption coefficient μ_a, by describing them using the mean pathlength L and variance σ^2.

$$\mu_a = \frac{1}{2L\sigma^2} \frac{L^2}{\sigma^2 + L^2} \qquad (5.3a)$$

$$\mu'_s \left[1 + \left(\frac{4}{3\mu'_s\rho}\right)\right] = \frac{2L}{3\rho^2} \left(1 + \frac{L^2}{\sigma^2}\right) \qquad (5.3b)$$

In the ordinary measurement, i.e., when $3\mu'_s\rho \gg 4$, the transport scattering coefficient can be approximated as follows.

$$\mu'_s = \frac{2L}{3\rho^2} \left(1 + \frac{L^2}{\sigma^2}\right) \qquad (5.4)$$

From the above, the transport scattering coefficient μ'_s and the absorption coefficient μ_a can be

30

quantified using the mean pathlength L and variance σ^2 computed from measured values. This method has the most significant feature and advantage of being simple and attains high accuracy for relatively large media, and the measurement accuracy of the transport scattering coefficient μ'_s and the absorption coefficient μ_a at this time is approximately 10%. However, this method presents excellent quantification accuracy for the ratio of transport scattering coefficients in measurement with different media or at different wavelengths. Namely, the transport scattering coefficient ratio can be measured with high accuracy and at high speed by the above method. In this case, the aforementioned subtraction method can be utilized for obtaining the mean pathlength L and variance σ^2.

Accordingly, the ratio of transport scattering coefficients obtained in measurement at the wavelengths λ_1 and λ_2, i.e., $\mu'_s(\lambda_2)/\mu'_s(\lambda_1)$, is given by the following equation, using the mean pathlengths L and variances σ^2 obtained in measurement at the respective wavelengths.

$$\frac{\mu'(\lambda_2)}{\mu'(\lambda_1)} \equiv \frac{\mu'_{s2}}{\mu'_{s1}} = \frac{L_2}{L_1}\frac{1+(L_2/\sigma_2)^2}{1+(L_1/\sigma_1)^2} \tag{5.5}$$

Therefore, aforementioned k' is given as follows.

$$k' = \left(\frac{\mu'_{s2}}{\mu'_{s1}}\right)^{1/2} = \left(\frac{L_2}{L_1}\frac{1+(L_2/\sigma_2)^2}{1+(L_1/\sigma_1)^2}\right)^{1/2} \qquad (5.6)$$

It is, however, noted that the mean pathlengths and variances are expressed by their abbreviations.

From the above, the absorber concentration C can be determined from measured values, by substituting Eq. (5.6) into Eq. (4.8). If the ratio of transport scattering coefficients is known, this known value may also be used. This ratio of transport scattering coefficients may also be gained by another method.

Preferred embodiments of the measuring methods and apparatus based on the above-stated measurement principles will be described below in detail.

(First Embodiment)

The first embodiment as a preferred embodiment of the present invention will be described with reference to Fig. 2 to Fig. 4. Fig. 2 shows a measuring system according to the present invention to quantify the concentration C of an absorber in a scattering medium 1, using light of two wavelengths. For simplicity of description, let us consider a liquid medium containing one absorber, in which the scattering and absorption characteristics are uniform. The liquid is, for example, water and it is necessary to take absorption of water in the measurement into consideration.

The apparatus illustrated in Fig. 2 is provided with a light guide 3 for injection of light and an output end of the light guide 3 is located at a predetermined position on the surface of the scattering medium 1. A light source 5 is optically coupled through a wavelength selector 4 to an input end of the light guide 3 and pulsed light emitted from the light source 5 is subjected to wavelength selection to the predetermined wavelength λ_1 and/or λ_2 in the wavelength selector 4. The light is then guided through the light guide 3 to be injected at the position u_j into the scattering medium 1.

The time width of this pulsed light can be set to any value short enough to derive the mean pathlength of the impulse response from a photodetection signal and is normally selected in the range of approximately 10 ps to 1 ns. The wavelengths of the light are properly selected according to the scattering medium 1 being a measured object and in general, for example, for living tissues, the wavelengths in the near infrared region of approximately 700 to 900 nm are normally used from the relation between transmittance of living tissue and spectral absorption coefficient of absorber to be quantified. The light source 5 can be selected from a variety of sources including light emitting diodes, laser diodes, various pulse lasers, and so on. This

light source 5 may be a combination of two or more
sources each emitting light of a single wavelength or
light of a narrow band, or may be one simultaneously
emitting light of two or more wavelengths. The
5   structure of the light guide 3 and wavelength selector
4 is also adequately modified or set according to the
structure of the light source 5 as described. The
light source may also be one time-sequentially
generating light of two or more wavelengths and in this
10 case the wavelength selector 4 can be omitted.

The apparatus illustrated in Fig. 2 is provided
with a light guide 6 for photodetection and an input
end of the light guide 6 is located at a predetermined
position on the surface of the scattering medium 1. A
15 photodetector 7 is optically coupled to an output end
of the light guide 6, and the light having propagated
with being scattered inside the scattering medium 1 is
guided from the position v_k through the light guide 6
to the photodetector 7. The photodetector 7 converts
20 the received signal into a photodetection signal being
an electric signal. A signal processing unit 8 is
electrically connected to the photodetector 7 and to
the light source 5 and this signal processing unit 8
acquires waveform data indicating temporal change of
25 intensity of detected light, based on the
photodetection signal. Further, an computation

34

processing unit 9 is electrically connected to the
signal processing unit 8 and this computation
processing unit 9 performs the operation to compute the
mean pathlength and variance of plural photons

5   constituting the detected light, based on the waveform
data. The absorption coefficient difference $(\mu_{a2} - \mu_{a1})$
is quantified according to aforementioned Eq. (4.8),
based on these mean pathlength, variance, and the ratio
of transport scattering coefficients at two wavelengths,

10 and the concentration C of the absorber is further
quantified according to aforementioned Eq. (4.9), based
on this absorption coefficient difference, or directly.

The light guide 3 for injection of light,
wavelength selector 4, and light source 5 described

15 above constitute the light injecting means according to
the present invention; the light guide 6 for detection
of light and the photodetector 7 the light detecting
means according to the present invention; and the
signal processing unit 8 the signal processing means

20 according to the present invention, respectively. The
computation processing unit 9 is configured with a
plurality of functions, which constitute the mean
pathlength and variance computing means (or the group
delay and second-partial-derivative-of-amplitude

25 computing means) and the absorption coefficient
difference calculating means according to the present

invention.

It is desirable to form the part except for the light injecting surface coupled to the light guide 3 and except for the light detecting surface coupled to the light guide 6 in the surface of the scattering medium 1, in structure in which light is absorbed inside but blocked outside. In the case wherein light of plural wavelengths simultaneously propagates with being scattered inside the scattering medium 1, a wavelength selecting filter (not illustrated) may be optionally placed between the photodetector 7 and the light guide 6 to carry out the measurement therewith.

Fig. 3 shows an example of preferred structure of the photodetector 7, signal processing unit 8, and computation processing unit 9. The setup illustrated in Fig. 3 is a configuration for carrying out a high-speed temporal profile measuring method using a method called so-called time-correlated single photon counting. In this setup example, a photomultiplier tube (PMT) is used as the photodetector 7 and the signal processing unit 8 is composed of a constant fraction discriminator (CFD) 21, a time-to-amplitude converter (TAC) 22, and an AD converter (A/D) 23. Then an output signal from the PMT 7 is guided through CFD 21 to TAC 22 to be converted into an analog voltage corresponding to time. This analog voltage is further converted into a digital

signal by the AD converter 23. This digital signal is one corresponding to waveform data indicating temporal change of intensity of detected light.

In the computation processing unit 9 illustrated in Fig. 3, a CPU 30 is electrically connected to the light source 5 and to the signal processing unit 8, the CPU 30 controls the timing of photodetection synchronized with injection of light and others, and the waveform data outputted from the signal processing unit 8 is guided to the CPU 30. This CPU 30 also controls or selects the wavelength of incident light and others. Specific techniques are a technique of injecting light of different wavelengths in time sharing manner and a technique of using light simultaneously containing beams of different wavelengths. Specific wavelength selecting means are, for example, an optical beam switch using a mirror, a wavelength switch using a filter, a light switch using an optical switch, and so on.

The computation processing unit 9 illustrated in Fig. 3 is further provided with a program memory 40 storing an operating system (OS) 41 and an internal information measuring program 42 detailed hereinafter, a data file memory 50 storing various data files, a data memory 61 storing data indicating obtained internal information of the scattering medium, a work

memory 62 temporarily saving working data, an input
device 70 with a keyboard 71 and a mouse 72 for
accepting entry of data, and an output device 80 with a
display 81 and a printer 82 for output of obtained data,
5   and these are also controlled by the CPU 30
electrically connected thereto. The above memories may
be configured in the form of an internal memory (hard
disk) of a computer or a flexible disk.

The data file memory 50 stores various data
10   including the waveform data, mean pathlength,
instrumental function (impulse response of the
measuring system), variance, ratio of transport
scattering coefficients, absorption coefficient
difference, etc. obtained by execution of the internal
15   information measuring program 42, and also stores the
data of measurement conditions, known values, etc.
preliminarily entered by use of the input device 70.
Such input data includes the shape of the measured
medium, the light injection position, the
20   photodetection position, the source-detector distance,
the wavelength of light used in the measurement, the
type of measurement (e.g., reflection type or
transmission type), the extinction coefficient at a
predetermined wavelength of the absorber as a measured
25   object, and so on.

The photodetector 7 can be selected from

photodetectors of various kinds, including photodiodes, avalanche photodiodes, PIN photodiodes, etc., as well as the photomultiplier tubes. For selection of the photodetector 7 to be used in the measurement, the

5   necessary condition is that it has spectral sensitivity characteristics capable of detecting re-emission of the wavelengths of the measurement light used. Further, it is preferable to use the photodetector with high sensitivity or with high gain if the photon signal is

10   weak. The source light guide 3 and the detector light guide 6 described above may also be replaced by optical fibers, lenses, or the like.

Next, the measuring method according to the present invention will be described below in detail on

15   the basis of the flowchart of an embodiment thereof illustrated in Fig. 4 (which is a flowchart indicating processing of the internal information measuring program 42 illustrated in Fig. 3).

In the flowchart illustrated in Fig. 4, the first

20   step is a step of injecting the pulsed light of a predetermined wavelength generated in the light source 5, through the light guide 3 into the scattering medium 1 at the light injection position u_j (S110) and the next step is a step of detecting the light having

25   propagated with being scattered inside the scattering medium 1, by the photodetector 7 through the light

guide 6 located at the photodetection position v_k
(S120).

Then the photodetector 7 outputs the
photodetection signal corresponding to the detected
5   light and the signal processing unit 8 converts it into
the waveform data indicating the temporal change of
intensity of detected light (S130). The instrumental
function (the impulse response of the measuring system)
is preliminarily measured (S190) and is stored in the
10   data file memory 50. On this occasion, the
instrumental function is measured in such a way that
the scattering medium 1 is removed from the structure
illustrated in Fig. 3 and the light output end of the
light guide 3 and the light input end of the light
15   guide 6 are directly opposed and coupled in contact to
each other. Therefore, the instrumental function
includes the influence of the pulse width of the light
source, the bandwidth of the detecting system, and so
on.

20   Then the mean pathlength L and the variance σ^2 of
plural photons constituting the impulse response are
computed, based on the obtained waveform data and
instrumental function (S140). The mean pathlength and
variance of the impulse response are the sum of the
25   mean pathlengths and the sum of the variances of the
measured profile and the instrumental function,

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respectively, as represented by aforementioned Eqs. (2.8) and (2.10). Since the mean pathlength is expressed by the weighted mean of time-resolved profile as indicated in aforementioned Eq. (1.2b) and the variance by aforementioned (1.3), they can be quickly obtained by computation based on the time-resolved profile, i.e., the waveform data obtained as above with the computer (computation of moment).

Then the square root of the ratio of scattering coefficients, i.e., k' is computed, based on the mean pathlength L and variance σ^2, in accordance with Eq. (5.6) (S150). Then the absorption coefficient difference of the scattering medium or the concentration of the absorber is calculated based on aforementioned Eq. (4.8) or based on Eq. (4.9), respectively (S160 or S170), and the result of the calculation is outputted (S180).

The above operation to compute the mean pathlength and variance (S140) may also be arranged to obtain the mean pathlength and variance from the impulse response obtained by the deconvolution operation of the waveform data with the instrumental function. In the above operation to compute the square root of the scattering coefficient ratio (S150), it is also possible to use a value preliminarily measured by another method, as described previously.

41

In the above embodiment, when the light of the predetermined wavelength is pulsed light of n + 2 (≥ 3, where n is an integer not less than 1) or more wavelengths, it is possible to determine n + 1

5 absorption coefficient differences and quantify concentrations of n + 1 absorbers from these values.

(Second Embodiment)

The present embodiment is an example of application of the present invention to the phase

10 modulation spectroscopy. In this case, the setup of the measuring system is one obtained by replacing the signal processing unit 8 described above and illustrated in Fig. 3, for example, with an computation unit including a lock-in amplifier. The light source 5

15 emits modulated light of two predetermined wavelengths λ_1 and/or λ_2 including three types of modulation frequency components $(\omega_1, \omega_2, \omega_3)$.

Fig. 5 is a flowchart of the embodiment in which the method of the present invention is applied to the

20 phase modulation spectroscopy. In the flowchart illustrated in Fig. 5, the first step is a step of injecting the intensity-modulated light of the predetermined wavelengths generated in the light source 5, through the light guide 3 into the scattering medium

25 1 at the light injection position u_j (S110) and the next step is a step of detecting the light having

42

propagated with being scattered inside the scattering medium 1, by the photodetector 7 through the light guide 6 located at the photodetection position v_k (S120). Then the photodetection signal corresponding to the detected light is outputted from the photodetector 7 to be supplied to the signal processing unit 8.

The lock-in amplifier included in the signal processing unit 8 extracts signals of the three predetermined frequency components from the modulated light of the wavelengths λ_1 and λ_2 described above (S131) and outputs the real parts R, imaginary parts X, amplitudes A, and phase delays ϕ stated in Eq. (3.1), about the signals of the three predetermined frequency components. The zero point of the phase is preliminarily acquired (S191). The next step in this embodiment is a step of computing the group delay of plural photons constituting the detected light of the modulation frequency of ω_2, and the second partial derivative of logarithm of amplitude with respect to ω (which is equal to the partial derivative of the group delay with respect to the absorption coefficient, see Eq. (3.5)), using the amplitudes A, phase delays ϕ, and three modulation frequencies (ω_1, ω_2, ω_3) of the signals of the three predetermined frequency components against injection of the modulated light of the two

43

predetermined wavelengths (S141).

Then the square root of the ratio of scattering
coefficients, i.e., k' is computed based on this group
delay and the partial derivative thereof with respect
to the absorption coefficient (S150). In this case,
the computation is carried out by replacing the mean
pathlength L with c times the group delay and replacing
the variance σ^2 with the second partial derivative of
logarithm of c^2 times the amplitude with respect to ω,
in aforementioned Eq. (5.6). Then the absorption
coefficient difference of the scattering medium, or the
concentration of the absorber is computed based on
aforementioned Eq. (4.8) or Eq. (4.9), respectively,
(S160 or S170) and the result of the computation is
outputted (S180). In these cases, however, the
computation is also conducted by replacing the mean
pathlength L with c times the group delay and replacing
the variance σ^2 with the second partial derivative of
logarithm of c^2 times the amplitude with respect to ω.

The above process is arranged to obtain the group
delay and the partial derivative thereof with respect
to the absorption coefficient, but in the case of $\omega \ll
c\mu_a$, the process may also be modified to compute the
phase delay and the partial derivative of the phase
delay with respect to the absorption coefficient,
because the group delay is approximated to the phase

44

delay in that case as described above. In the above operation to compute the square root of the ratio of scattering coefficients (S150), it is also possible to use a value preliminarily measured by another method.

In the above embodiment, when the light of the predetermined wavelengths is pulsed light of n + 2 ($\geq$ 3, where n is an integer not less than 1) or more wavelengths, it becomes feasible to obtain n + 1 absorption coefficient differences and quantify concentrations of n + 1 absorbers from these values.

(Third Embodiment)

Fig. 6 shows the third embodiment of the present invention to illustrate a system for measuring or monitoring the concentration of hemoglobin or oxygen saturation of hemoglobin inside a scattering medium such as a human head. This system uses light of three wavelengths, i.e., wavelengths λ_1, λ_2, and λ_3. In this case, the operation principle and structure are the same as in the first embodiment with use of pulsed light and the same as in the second embodiment with use of modulated light. The system of the present embodiment, however, is different in the structure of a container housing the light injecting means and light detecting means from each of the above embodiments.

In the system illustrated in Fig. 6, the light injecting means and light detecting means are housed in

45

the container 10 provided with a fitting band to be
mounted on the head 1a like a headband and are
connected through a cable 12 to an external device 11
including the signal processing unit 8, the computation

5   processing unit 9, and so on.

Fig. 7 shows the details of the container 10.
The container 10 incorporates the light source 5,
wavelength selector 4, source light guide 3, detector
light guide 6, and photodetector 7. The light of the

10   predetermined wavelengths λ_1, λ_2, λ_3 emitted from the
light source 5 is subjected to the wavelength selection
in the wavelength selector 4 and light of the selected
wavelength is guided through the light guide 3 into the
head 1a. On this occasion, the predetermined

15   wavelengths λ_1, λ_2, and λ_3 are properly selected with
reference to the absorption spectrum of hemoglobin
illustrated in Fig. 8.

The above system is constructed in such structure
that the cable 12 connects the container 10

20   incorporating the light injecting means and light
detecting means, via a connector 13 with the external
device 11 housing the signal processing unit 8 and the
computation processing unit 9, but the system may also
be constructed so as to connect them with each other by

25   another means such as wireless communication, optical
signals, or the like. Such arrangement permits, for

example, not only measurement on the bed side or in a state of repose, but also measurement in a state of motion. Besides the head, it is also possible to implement measurement with an object such as the thigh

5   or the like of a marathon runner during a race, for example. Further, if the system is connected to a city cable, an optical cable, or the like, it will also become feasible to implement remote measurement for a person at home from facilities such as hospitals or the

10 like and to apply it to centralized control or the like of patient rooms in the hospitals, for example.

Here let us denote the concentrations and optical constants of hemoglobin as follows.

C_b: molar concentration (M) of deoxygenated

15 hemoglobin,

C_o: molar concentration (M) of oxygenated hemoglobin,

p_1: molar extinction coefficient ($mm^{-1}M^{-1}$) at the wavelength λ_1 of deoxygenated hemoglobin,

20 p_2: molar extinction coefficient ($mm^{-1}M^{-1}$) at the wavelength λ_2 of deoxygenated hemoglobin,

p_3: molar extinction coefficient ($mm^{-1}M^{-1}$) at the wavelength λ_3 of deoxygenated hemoglobin,

q_1: molar extinction coefficient ($mm^{-1}M^{-1}$) at the

25 wavelength λ_4 of oxygenated hemoglobin,

q_2: molar extinction coefficient ($mm^{-1}M^{-1}$) at the

wavelength λ_5 of oxygenated hemoglobin,

q_3: molar extinction coefficient $(mm^{-1}M^{-1})$ at the wavelength λ_6 of oxygenated hemoglobin

Then the absorption coefficients at the respective

5   wavelengths are expressed as follows.

$$\mu_{a1} = p_1 C_b + q_1 C_o + a_1$$
$$\mu_{a2} = p_2 C_b + q_2 C_o + a_2$$
$$\mu_{a3} = p_3 C_b + q_3 C_o + a_3 \qquad (A1.1)$$

In these equations, a_1, a_2, and a_3 are absorption coefficients of water and the absorbers other than hemoglobin.

10   Since values actually measured by the method of the present invention are absorption coefficient differences, the above equations are rewritten as follows corresponding thereto.

$$\mu_{a2} - \mu_{a1} = (p_2 - p_1)C_b + (q_2 - q_1)C_o + a_2 - a_1$$
$$\mu_{a3} - \mu_{a1} = (p_3 - p_1)C_b + (q_3 - q_1)C_o + a_3 - a_1 \qquad (A1.2)$$

15   Namely, the left sides of the above equations are quantities measured by the method of the present invention. Since these equations are simultaneous equations including two unknowns C_b and C_o, the two unknowns C_b and C_o can be determined by solving these

20   simultaneous equations. In this case, as to values of a_1, a_2, and a_3, the wavelengths are normally selected so as to make $a_1 \fallingdotseq a_2 \fallingdotseq a_3$. It is also possible to use standard values of living tissues for the values of a_1,

a_2, a_3.

According to the above, this embodiment allows us to determine the concentration C_b of deoxygenated hemoglobin, the concentration C_o of oxygenated hemoglobin, the amount of hemoglobin $(C_b + C_o)$, and the oxygen saturation $C_o/(C_b + C_o)$.

The above described the preferred embodiments of the present invention, but it is noted that the present invention is by no means limited to the above embodiments, of course.

Specifically, the light injection position and photodetection position are fixed in the above embodiments, but the light injection position and/or the photodetection position may be moved to scan. It can also be contemplated that a plurality of light injection positions and/or photodetection positions are arranged around the scattering medium.

Further, in the above embodiments the scattering characteristics during measurement can be considered to be constant when the measurement is carried out with moving the light injection position and/or the photodetection position relative to one scattering medium, or when the measurement is carried out at a fixed position of a scattering medium before and after change in the concentration of an absorber. In this case, a concentration distribution of an absorber

(differences with respect to a reference value) or a
concentration change of an absorber (differences with
respect to a reference value) can be measured by
setting k' = 1 in aforementioned Eq. (4.9) and Eq.

5   (4.10). Particularly, the former example is effective,
for example, to the measurement in Example 2
(mammography) disclosed in Japanese Patent Application
Laid-Open No. H10-73481 by the inventors of the present
application.

10   The present invention will be described in
further detail on the basis of examples.
(Example 1)
      The present example provides the results of
simulation performed for confirming the accuracy of the

15   method of the present invention.
      Specifically, Monte Carlo simulation was
conducted as to the spectroscopy using the mean
pathlength and variance according to the present
invention (the MVS method) with variation of absorption

20   coefficient for slablike scattering media (media)
having the thickness of 30 mm. Although this Monte
Carlo simulation does not present data directly
corresponding to data measured by dual-wavelength
spectroscopy, it allows simulation of validity of the

25   dual-wavelength spectroscopy, using Monte Carlo data at
different concentrations of an absorber. Namely,

aforementioned Eq. (4.8) with k' = 1 is applied to quantification of the difference between absorption coefficients.

Table 1 and Table 2 present the results of measurement with the source-detector distance of 5 mm in the reflection measurement and Table 3 and Table 4 the results of measurement with the source-detector distance of 30 mm in the reflection measurement. Table 5 and Table 6 present the results of measurement with the source-detector distance of 30 mm (corresponding to the thickness of the medium) in the transmission measurement. The scattering coefficient $\mu'_s = 1mm^{-1}$ in all the cases, but the mean cosine of scattering angles is g = 0.6 in Tables 1, 3, and 5 and g = 0.9 in the Tables 2, 4, and 6.

TABLE 1

μ_a	L	σ	$\Delta\mu_a$	Error (%)	Old-$\Delta\mu_a$	Error (%)
0.005	26.063	31.90	-----	-----	-----	-----
0.01	22.98	23.15	0.0047	−6	0.0053	6
0.02	19.30	16.17	0.0092	−8	0.0111	11
0.03	17.23	12.91	0.0097	−3	0.0114	14

TABLE 2

μ_a	L	σ	$\Delta\mu_a$	Error (%)	Old-$\Delta\mu_a$	Error (%)
0.005	26.19	31.58	-----	-----	-----	-----
0.01	22.62	22.91	0.0047	−6	0.0053	6
0.02	19.00	15.99	0.0093	−7	0.0111	11
0.03	16.98	12.76	0.0097	−3	0.0116	16

TABLE 3

μ_a	L	σ	$\Delta\mu_a$	Error (%)	Old-$\Delta\mu_a$	Error (%)
0.005	283.50	137.56	-----	-----	-----	-----
0.01	219.51	93.43	0.0046	−8	0.0046	−8
0.02	165.16	59.20	0.0089	−11	0.0102	2
0.03	138.77	44.44	0.0096	−4	0.0110	10

TABLE 4

μ_a	L	σ	$\Delta\mu_a$	Error (%)	Old-$\Delta\mu_a$	Error (%)
0.005	284.02	137.65	-----	-----	-----	-----
0.01	219.75	93.32	0.0046	− 8	0.0046	−8
0.02	165.44	59.03	0.0089	−11	0.0104	4
0.03	139.39	44.40	0.0095	− 5	0.0110	10

TABLE 5

μ_a	L	σ	$\Delta\mu_a$	Error (%)	Old-$\Delta\mu_a$	Error (%)
0.005	231.94	110.03	-----	-----	-----	-----
0.01	190.39	78.01	0.0046	− 8	0.0056	12
0.02	150.92	51.83	0.0090	−10	0.0117	17
0.03	129.03	40.63	0.0101	1	0.0104	4

TABLE 6

μ_a	L	σ	$\Delta\mu_a$	Error (%)	Old-$\Delta\mu_a$	Error (%)
0.005	232.00	110.23	-----	-----	-----	-----
0.01	190.29	77.74	0.0044	−12	0.0057	14
0.02	150.39	52.05	0.0091	− 9	0.0113	13
0.03	129.18	40.22	0.0098	− 2	0.0116	16

10   In each of the tables μ_a in the left extreme

column represents the absorption coefficients of media

set on the occasion of Monte Carlo calculation. In the

tables $\Delta\mu_a$ in the central part represents the

absorption coefficient differences quantified by
aforementioned Eq. (4.8), using the mean pathlengths L
and variances σ^2 computed from a set of Monte Carlo
data of upper and lower neighbors. However, k' = 1.

5   In the tables the right part presents Old-$\Delta\mu_a$ to
indicate the absorption coefficient differences
obtained by another method for quantifying the ratio of
transport scattering coefficients (Eq. (5.3a)) for
comparison. From the tables, this Old-$\Delta\mu_a$ shows a

10   tendency of DC biasing in the reflection measurement
and a tendency of the slope becoming larger than 1 in
the transmission measurement, and $\Delta\mu_a$ obtained by the
method according to the present invention demonstrates
smaller errors than Old-$\Delta\mu_a$.

15   The smaller the absorption coefficient μ_a, the
larger the change of slope of mean pathlength L against
absorption coefficient μ_a becomes (see Fig. 1).
Therefore, there arises the error of linear
approximation (equivalent to use of the mean value

20   theorem) used for deriving aforementioned Eq. (1.5), in
the small region of the absorption coefficient μ_a. Of
course, this error decreases with decrease in the
absorption coefficient difference. This tendency is
seen in the results of Table 1 to Table 6 and the

25   quantified values in the bottom row show considerably
good accuracy. In the spectroscopy of actual living

tissues or the like, the difference between absorption
coefficients at two wavelengths becomes small just when
the absorption coefficient μ_a is small, as described
hereinafter. Since the living tissues involve the

5   absorption of water, absolute values of absorption
coefficients also become larger by that degree.
Accordingly, these two points largely relax the above
error in the spectroscopy of living tissues or the like.
(Example 2)

10   The present example provides the results of
experiments conducted with a simulated phantom in order
to confirm the accuracy of the method of the present
invention.

         The schematic structure of the experimental setup

15   was as illustrated in Fig. 3, and the light source was
two picosecond pulse generators that generated
picosecond pulses of the respective wavelengths $\lambda_1 =$
782 nm and $\lambda_2 = 831$ nm, the repetition rate of 5 MHz,
and the pulse width of about 50 ps. These picosecond

20   pulses are injected through an optical switch and an
optical attenuator into a GI fiber having the diameter
of 200 μm and light emerging from an output end being
the other end of the fiber is injected into the phantom
being a scattering medium. Output light from the

25   phantom is received by a bundle fiber having the
diameter of 5 mm and is measured by the system based on

the time-correlated single photon counting method as illustrated in Fig. 3. The instrumental functions at the two wavelengths necessary for the computation of mean pathlength are measured with the light injection and photodetection fibers kept in a closely fitted state.

The phantom used in the experiments was prepared by putting 420 ml of a 1% intralipid solution as a scattering substance into an acrylic vessel (width 120 mm, height 120 mm, and depth 40 mm) and gradually adding greenish brown ink 0.07 ml every time as an absorbing substance to the solution until the total amount of the ink became 0.56 ml, and the transmission measurement was carried out under the condition of the source-detector distance of 40 mm. The actual absorption coefficient of the phantom is the sum of the absorption coefficient of the added ink and the absorption coefficient of water (distilled water). At the wavelengths λ_1 = 782 nm and λ_2 = 831 nm of the pulsed light used in the measurement, theoretical values of the transport scattering coefficient are 1.0207 and 0.9531, respectively. Therefore, a ratio of them is 1.071 and k' = 1/1.035 = 0.9633. The extinction coefficient of greenish brown ink and the absorption coefficient of distilled water were measured by a spectroscope. Table 7 presents the optical

parameters of the phantom in the experiments.

TABLE 7

Wavelength (nm)	$\lambda_1 = 782$	$\lambda_2 = 831$	Difference between or ratio of coefficients at the wavelengths
Absorption coefficient of water (mm^{-1})	$\mu_{w1} =$ 2.452×10^{-3}	$\mu_{w2} =$ 3.095×10^{-3}	$\mu_{w2} - \mu_{w1} =$ 0.643×10^{-3}
Extinction coefficient (mm$^{-1} \cdot$ml^{-1})	$\varepsilon_1 = 4.806 \times 10^{-2}$	$\varepsilon_2 = 2.758 \times 10^{-2}$	$\varepsilon_2 - \varepsilon_1 = -2.048 \times 10^{-2}$
Transport scattering coefficient (mm^{-1})	$\mu_{s1} = 1.0207$	$\mu_{s2} = 0.9531$	$(\mu_{s2}/\mu_{s1})^{1/2} = 0.9633$

Table 8 presents values of the mean pathlength and variance of the impulse response calculated from experimental values obtained in the experiments with the phantom carried out under the above conditions.

TABLE 8

Ink (ml)	$L(\lambda_1)$ (×10^2 mm)	$L(\lambda_2)$ (×10^2 mm)	$\sigma^2(\lambda_1)$ (×10^4 mm)	$\sigma^2(\lambda_2)$ (×10^4 mm)
0.00	4.2007	3.8468	3.5658	2.9339
0.07	3.3142	3.3683	1.6680	1.8673
0.14	2.8670	3.0533	1.0439	1.3639
0.21	2.5690	2.8141	0.7275	1.0329
0.28	2.3322	2.6051	0.5572	0.8342
0.35	2.1610	2.4412	0.4399	0.6946
0.42	2.0367	2.3369	0.3605	0.5910
0.49	1.9164	2.2304	0.2993	0.5125
0.56	1.8336	2.1266	0.2611	0.4546

The absorption of water is unignorable in the measurement with the living tissues and living-tissue-

simulated liquid phantoms. The extinction coefficient
of an absorber differs depending upon wavelengths, and
the spectroscopy makes use of this difference. Fig. 9
shows the relation between absorption coefficient and
mean pathlength of a phantom. In this relation the
absorption coefficients of the phantom were calculated
using the absorption coefficient of distilled water
actually measured, the quantity of added ink, and the
extinction coefficient of ink actually measured. The
curves in the figure are the results of fitting in the
general form of the following equation indicating the
mean photon pathlength obtained by the photon diffusion
approximation.

$$L = 1 / \left(a + b \sqrt{\mu_a} \right)$$

It is seen from this Fig. 9 that Eq. (4.6)
approximately holds.

Further, it is also seen that, considering the
absorption coefficient difference in a set of data used
in the spectroscopy in the figure, i.e., in a set of
data at the same quantity of added ink, this difference
increases with increase in the absorption coefficient
of the phantom and the difference also becomes smaller
with decrease in the absorption coefficient of the
phantom. This relation generally holds for the
spectroscopy of living tissues or the like. The linear

approximation was used for deriving Eq. (1.5) being the
fundamental equation of the MVS method. Since the
curvature of mean pathlength and the absorption
coefficient difference are just in the relation of one
5   increasing with decrease of the other, as illustrated
in Fig. 9, it is seen that the linear approximation
holds with small error throughout the entire region of
change of the absorption coefficient.

     Concentrations C of the absorber quantified by
10   the experiments are presented in Table 9. For
comparison's sake, Table 9 also presents the results by
the method using a fixed value for the ratio k' (k' =
0.9663, which is a theoretical value), the results on
the assumption that the transport scattering
15   coefficient has no wavelength dependence (k' = 1), and
the results by use of an average of the ratios of
transport scattering coefficients obtained by the
experiments (k' = 0.9681). It is apparent from this
table that the errors are naturally large on the
20   assumption that the transport scattering coefficient
has no wavelength dependence (k' = 1) and that the
method according to the present invention assures
excellent accuracy as against the other methods.

     As compared with the results by use of the
25   average of the ratios gained by the experiments (k' =
0.9681), the results with k' obtained in each

measurement show smaller errors, and this is
conceivably because the influence of noise in each
measurement is canceled out in the process of operation.

TABLE 9

Ink (ml)	Method of the invention			$k' = 0.9663$		$k' = 1$		$k' = 0.9681$	
	k'	C (ml)	Error (%)	$C_{k'2}$ (ml)	Error (%)	$C_{k'1}$ (ml)	Error (%)	$C_{k'3}$ (ml)	Error (%)
0.00	0.9646	−0.000	--	−0.001	--	−0.022	--	−0.002	--
0.07	0.9737	0.071	1.4	0.078	11.4	0.046	−34	0.076	8.5
0.14	0.9697	0.144	2.9	0.148	5.7	0.107	−24	0.146	4.3
0.21	0.9709	0.211	0.5	0.218	3.8	0.168	−20	0.216	2.9
0.28	0.9738	0.269	−3.9	0.282	0.7	0.223	−20	0.279	−0.4
0.35	0.9652	0.342	−2.3	0.340	−2.9	0.273	−22	0.337	−3.7
0.42	0.9693	0.409	−2.6	0.416	−1.0	0.340	−19	0.412	−1.9
0.49	0.9690	0.487	−0.6	0.494	0.8	0.410	−16	0.489	−0.2
0.56	0.9566	0.549	−2.0	0.520	−7.1	0.432	−23	0.518	−7.5

Industrial Applicability

The measuring methods and apparatus of internal
information of scattering medium according to the
present invention are applicable to measurement of the
absorption coefficient of the scattering medium and the
concentration of the absorber, as measuring methods and
apparatus of internal information of scattering medium
capable of measurement with higher accuracy and at
higher speed than the conventional measuring methods
based on the MBL law. Particularly, the measuring
methods and apparatus according to the present
invention make use of the mean pathlength and variance,

or physical quantities equivalent thereto, but do not make use of information of the absolute value of light intensity or the ratio thereof. Accordingly, they are useful in that a solution is given to the difficult problem in practical use; quantifying or estimating the absolute value of quantity of light injected into the medium.

Such methods make real-time measurement feasible and also possess the great feature that the measurement can be conducted independent of the shape and boundary conditions, the size of the medium, the scattering characteristics, the source-detector distance, the measurement mode of either transmission or reflection, and so on. From the above, the measuring methods and apparatus of internal information of scattering medium according to the present invention are expected to be commonly applied to apparatus for simply measuring various physiological substances in living tissues on a noninvasive and real-time basis.